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Name: Jodi Jung

SPECIFICATION

TO ALL WHOM IT MAY CONCERN:

BE IT KNOWN THAT WE, Patrick M. McCarthy, a citizen of the United
States of America, and a resident of Hunting Valley, Ohio, Cyril J. Schweich,
Jr., a citizen of the United States of America, and a resident of St. Paul,
Minnesota, Todd J. Mortier, a citizen of the United States of America, and a
resident of Minneapolis, Minnesota, Peter T. Keith, a citizen of the United States
of America, and a resident of St. Paul, Minnesota, and Michael J. Kallok, a
citizen of the United States of America, and a resident of New Brighton,
Minnesota, have invented certain new and useful improvements in

**METHODS AND DEVICES FOR IMPROVING
CARDIAC FUNCTION IN HEARTS**

of which the following is a specification.

METHODS AND DEVICES FOR IMPROVING CARDIAC FUNCTION IN HEARTS

This application is a continuation of U.S. Patent Application Serial No.
5 10/136,446 filed May 2, 2002, now pending, which is a continuation of
09/422,328 filed October 21, 1999, now U.S. Patent No. 6,406,420, issued June
18, 2002, which is a continuation-in-part of U.S. Patent Application Serial No.
09/124,286 filed July 29, 1998, now U.S. Patent No. 6,045,497, issued April 4,
2000, which is a continuation-in-part of U.S. Patent Application Serial No.
10 08/933,456 filed September 18, 1997, now U.S. Patent No. 5,961,440, issued
October 5, 1999, which is a continuation-in-part of U.S. Patent Application
Serial No. 08/778,277, filed January 2, 1997, now U.S. Patent No. 6,050,936,
issued April 18, 2000.

15

FIELD OF THE INVENTION

The present invention pertains to the field of apparatus for treatment of a
failing heart. In particular, the apparatus and its related methods of the present
invention is directed toward reducing the wall stress in the failing heart. The
present invention further includes methods and devices for improving cardiac
20 function in hearts having discrete zones of infarcted tissue. Such methods and
devices reduce the radius of curvature and/or alter the geometry or shape of the
infarcted tissue and adjacent regions to thereby reduce wall stress on the heart
and improve the heart's pumping performance.

25

BACKGROUND OF THE INVENTION

The syndrome of heart failure is a common course for the progression of
many forms of heart disease. Heart failure may be considered to be the condition
in which an abnormality of cardiac function is responsible for the inability of the
heart to pump blood at a rate commensurate with the requirements of the
30 metabolizing tissues, or can do so only at an abnormally elevated filling pressure.
There are many specific disease processes that can lead to heart failure. Typically
these processes result in dilatation of the left ventricular chamber. Etiologies that

can lead to this form of failure include idiopathic, valvular, viral, and ischemic cardiomyopathies.

The process of ventricular dilatation is generally the result of chronic volume overload or specific damage to the myocardium. In a normal heart that is exposed to long term increased cardiac output requirements, for example, that of an athlete, there is an adaptive process of slight ventricular dilation and muscle myocyte hypertrophy. In this way, the heart fully compensates for the increased cardiac output requirements. With damage to the myocardium or chronic volume overload, however, there are increased requirements put on the contracting myocardium to such a level that this compensated state is never achieved and the heart continues to dilate.

The basic problem with a large dilated left ventricle is that there is a significant increase in wall tension and/or stress both during diastolic filling and during systolic contraction. In a normal heart, the adaptation of muscle hypertrophy (thickening) and ventricular dilatation maintain a fairly constant wall tension for systolic contraction. However, in a failing heart, the ongoing dilatation is greater than the hypertrophy and the result is a rising wall tension requirement for systolic contraction. This is felt to be an ongoing insult to the muscle myocyte resulting in further muscle damage. The increase in wall stress is also true for diastolic filling. Additionally, because of the lack of cardiac output, there is generally a rise in ventricular filling pressure from several physiologic mechanisms. Moreover, in diastole there is both a diameter increase and a pressure increase over normal, both contributing to higher wall stress levels. The increase in diastolic wall stress is felt to be the primary contributor to ongoing dilatation of the chamber.

Prior treatments for heart failure associated with such dilatation fall into three general categories. The first being pharmacological, for example, diuretics and ACE inhibitors. The second being assist systems, for example, pumps. Finally, surgical treatments have been experimented with, which are described in more detail below.

With respect to pharmacological treatments, diuretics have been used to reduce the workload of the heart by reducing blood volume and preload. Clinically, preload is defined in several ways including left ventricular end diastolic pressure (LVEDP), or indirectly by left ventricular end diastolic volume (LVEDV). Physiologically, the preferred definition is the length of stretch of the sarcomere at end diastole. Diuretics reduce extra cellular fluid which builds in congestive heart failure patients increasing preload conditions. Nitrates, arteriolar vasodilators, angiotensin converting enzyme (ACE) inhibitors have been used to treat heart failure through the reduction of cardiac workload by reducing afterload. Afterload may be defined as the tension or stress required in the wall of the ventricle during ejection. Inotropes function to increase cardiac output by increasing the force and speed of cardiac muscle contraction. These drug therapies offer some beneficial effects but do not stop the progression of the disease.

Assist devices include mechanical pumps. Mechanical pumps reduce the load on the heart by performing all or part of the pumping function normally done by the heart. Currently, mechanical pumps are used to sustain the patient while a donor heart for transplantation becomes available for the patient.

There are at least four surgical procedures for treatment of heart failure associated with dilatation: 1) heart transplantation; 2) dynamic cardiomyoplasty; 3) the Batista partial left ventriculectomy; and 4) the Jatene and Dor procedures for ischemic cardiomyopathy, discussed in more detail below. Heart transplantation has serious limitations including restricted availability of organs and adverse effects of immunosuppressive therapies required following heart transplantation. Cardiomyoplasty involves wrapping the heart with skeletal muscle and electrically stimulating the muscle to contract synchronously with the heart in order to help the pumping function of the heart. The Batista partial left ventriculectomy surgically remodels the left ventricle by removing a segment of the muscular wall. This procedure reduces the diameter of the dilated heart, which in turn reduces the loading of the heart. However, this extremely invasive procedure reduces muscle mass of the heart.

One form of heart failure, ischemic cardiomyopathy, results from the formation of one or more zones of ischemia, or infarction, of the myocardium. Infarction occurs when blood supply to the heart tissue has been obstructed resulting in a region of tissue that loses its ability to contract (referred to as infarcted tissue). The presence of infarcted tissue may lead to three conditions in the heart causing cardiac malfunction. These conditions are ventricular aneurysms (ventricular dyskinesia), non-aneurysmal ischemic or infarcted myocardium (ventricular akinesia), and mitral regurgitation.

Ventricular aneurysms typically result from a transmural myocardial infarction, frequently due to the occlusion of the left anterior descending artery (LAD). This results in a transmural infarcted region of the apical portion of the left ventricle and anterior septal. A ventricular aneurysm is formed when the infarction weakens the heart wall to such an extent that the tissue stretches and thins, causing the left ventricular wall to expand during systole (dyskinesia). Figure 55 illustrates a ventricular aneurysm A occurring in the apical region of left ventricle LV. As shown by the shaded region in Figure 55, aneurysm A includes infarcted tissue 24 that results in a reduced wall thickness when compared to adjacent non-infarcted wall regions, as shown by the unshaded regions in Figure 55. Figure 55 also shows the septal wall S partially infarcted, again shown by the shaded region. The ventricular aneurysm also may be dyskinetic, meaning that when the ventricle contracts, the aneurysm further dilates, or bulges, outward. The infarcted region of the septal wall S also may be particularly dyskinetic, especially in the case of the infarcted tissue having progressed to an aneurysm.

The bulge resulting from an aneurysm can have several serious effects on the heart and its performance that can lead to in both morbidity and mortality. For example, because the bulge creates a geometric abnormality as well as a region of non-contracting tissue, thrombosis is more likely to occur in that region. Thrombosis is the formation of a blood clot, or thrombus, that can cause other medical complications, such as a stroke. An ischemic stroke is a blockage

of blood flow to the brain that occurs when the thrombus breaks free and is ejected out of the ventricle.

Another serious effect this bulging can have is the denigration of the heart's pumping function. The aneurysmal bulge creates problems with pumping
5 function in at least three ways. First, the infarcted tissue does not contribute to the pumping of the ventricle because it does not contract (akinesia). To account for this loss of pumping, remaining portions of the ventricle wall may contract more to maintain cardiac output. If the infarcted region thins and progresses to an aneurysm (dyskinesia), this effect is further exacerbated by the aneurysm
10 expanding with a portion of the blood from the ventricular contraction. This further increases the contractile requirement of the remaining functional myocardium.

Second, the aneurysmal bulge alters the geometry of the entire ventricular chamber. Thus the ventricle develops a larger radius of curvature, which
15 directly applies more tension to the heart wall, as characterized by LaPlace's law.

Third, over time, the above two conditions lead the functional muscle of the ventricle to work harder than normal. This can lead to continued dilatation of the ventricle, increasing tension in the walls of the heart, with increased myocardial oxygen requirement and further progressing heart failure.

20 Non-aneurysmal ischemic or infarcted myocardium (akinesia) occurs when a major coronary artery is occluded and results in infarction in the myocardial tissue, but without a bulging aneurysm. In a manner similar to an aneurysm, the akinetic ischemic or infarcted zone ceases to participate in the ventricular contraction. This results in the functioning, contractile myocardium
25 needing to contract more to make up for the lack of contraction of the akinetic zone. Typically, the result is the entire ventricle increasing in size, which increases wall stress. Again, since the functioning myocardium must work harder, continuing progression of heart failure can occur.

Mitral regurgitation also may result from infarcted tissue, depending on
30 the region of the ventricle that has become infarcted or aneurysmal and any subsequent overall ventricular dilation. Mitral regurgitation is a condition

whereby blood leaks through the mitral valve due to an improper positioning of the valve structures that causes it not to close entirely. If the infarcted or aneurysmal region is located in the vicinity of the mitral valve, geometric abnormalities may cause the mitral valve to alter its normal position and dimension, and may lead to annular dilatation and the development of mitral regurgitation.

Typical treatments of infarcted tissue, and ventricular aneurysms in particular, include a variety of open surgical procedures. In the case of a ventricular aneurysm, traditionally, a "linear" aneurysmectomy is performed.

This procedure involves the removal of aneurysmal portions of the anterior wall along with any thrombus that may exist. Figure 41 illustrates the result of a conventional surgical method when an aneurysm occurs in the distal left ventricle. According to this method, the region of aneurysmal scar tissue that extends through the entire thickness of the chamber wall (transmural infarction) is removed by incision and the remaining border zone regions 24' (i.e., regions where infarcted tissue meets non-infarcted muscle) are sewn together with a suture 27. In a linear aneurysm repair procedure, the ventricular septal wall S that is infarcted is left untouched. Additionally, the septal wall generally remains untouched because simple excision and suturing does not involve excluding or cutting the septal wall. Usually, only those wall portions having infarcted tissue through their thickness (transmural infarcted) are removed while the portions having infarcted tissue only on an inner wall (endocardial infarcted) are left in place. The term border zone refers to this region of endocardial infarction. This surgical procedure results in some infarcted tissue regions remaining in the heart chamber, particularly any infarcted tissue in the septal wall. The effects of the remaining non-contractile tissue stresses the remaining contractile tissue because this contractile tissue must "make up" for the non-contracting and often dyskinetic tissue. Over time, these effects can continue to lead to progression of heart failure.

These procedures have to be performed with the patient on cardiopulmonary bypass. The heart also may be stopped in order to perform the

surgery. Any thrombus inside the ventricle is removed. Clinical results of this traditional surgical procedure have been mixed with respect to improvement in cardiac function.

Newer surgical approaches include the "Dor" and "Jatene" procedures. In the "Dor" procedure, the aneurysm is removed and an endocardial patch is placed to cover the dyskinetic septal wall portion of the aneurysm. In this manner, at least the portion of stroke volume "lost" to dyskinesia is restored. In the "Jatene" technique, a purse string suture is placed at the base of the aneurysm. The infarcted septal wall is circumferentially reduced by inbrication with sutures. The result is that most of the aneurysmal tissue is excluded from the ventricle. These procedures address the infarcted septal wall, generally left untouched in the traditional linear aneurysmectomy, by either exclusion or by the use of a surgical patch. These newer techniques are also used in cases of non-aneurysmal infarctions (akinesia). In these cases, the exclusion or elimination of the infarcted region reduces the size and therefore the radius of the chamber, thereby lowering wall stress.

These various described techniques for treating infarcted and aneurysmal tissue regions in the heart wall suffer from limitations and drawbacks. For instance, many of the surgical techniques involve invasive incisions in the heart wall which can be traumatic and risky to patients. Also, while these procedures attempt to improve cardiac function by removal of the aneurysm or infarcted tissue, they only minimally reduce the wall stress of the remaining contractile ventricle. Furthermore, patients typically undergo cardiopulmonary bypass and/or their heart is stopped during many of these surgeries.

25

SUMMARY OF THE INVENTION

The advantages and purpose of the invention will be set forth in part in the description which follows, and in part will be obvious from the description, or may be learned by practice of the invention. The advantages and purpose of the invention will be realized and attained by means of the elements and combinations particularly pointed out in the appended claims.

30

Due to the drawbacks and limitations of the previous techniques for treating dilated, infarcted, and aneurysmal tissue in hearts, there exists a need for alternative methods and devices that are less invasive, pose less risk to the patient, and are likely to prove more clinically effective. The present invention
5 provides improvements in these areas over the existing techniques.

One aspect of the present invention pertains to a non-pharmacological, passive apparatus and method for the treatment of a failing heart due to dilatation. The device is configured to reduce the tension in the heart wall. It is believed to reverse, stop or slow the disease process of a failing heart as it
10 reduces the energy consumption of the failing heart, decreases isovolumetric contraction, increases isotonic contraction (sarcomere shortening), which in turn increases stroke volume. The device reduces wall tension during diastole and systole.

These apparatus of the present invention which reduce heart wall stress
15 by changing chamber wall geometry can be referred to as "splints". Splints can be grouped as either "full cycle splints," which engage the heart to produce a chamber shape change throughout the cardiac cycle, or "restrictive splints," which do not engage the heart wall at end systole to produce a chamber shape change.

20 In one embodiment, the apparatus includes a tension member for drawing at least two walls of the heart chamber toward each other to reduce the radius or area of the heart chamber in at least one cross sectional plane. The tension member has anchoring members disposed at opposite ends for engagement with the heart or chamber wall.

25 In another embodiment, the apparatus includes a compression member for drawing at least two walls of a heart chamber toward each other. In one embodiment, the compression member includes a balloon. In another embodiment of the apparatus, a frame is provided for supporting the compression member.

30 Yet another embodiment of the invention includes a clamp having two ends biased toward one another for drawing at least two walls of a heart chamber

toward each other. The clamp includes at least two ends having atraumatic anchoring members disposed thereon for engagement with the heart or chamber wall.

5 In yet another embodiment, a heart wall tension reduction apparatus is provided which includes a first tension member having two oppositely disposed ends and first and second elongate anchor members. A second tension member can be provided. One of the elongate anchors may be substituted for by two smaller anchors.

10 In an alternate embodiment of the heart wall tension reduction apparatus, an elongate compression member can be provided. First and second elongate lever members preferably extend from opposite ends of the compression member. A tension member extends between the first and second lever members.

15 The compression member of the above embodiment can be disposed exterior to, or internally of the heart. The tension member extends through the chamber or chambers to bias the lever members toward the heart.

In yet another embodiment of a heart wall tension reduction apparatus in accordance with the present invention, a rigid elongate frame member is provided. The frame member can extend through one or more chambers of the heart. One or more cantilever members can be disposed at opposite ends of the frame member. Each cantilever member includes at least one atraumatic pad disposed thereon. The atraumatic pads disposed at opposite ends of the frame member can be biased toward each other to compress the heart chamber.

25 One method of placing a heart wall tension apparatus or splint on a human heart includes the step of extending a hollow needle through at least one chamber of the heart such that each end of the needle is external to the chamber. A flexible leader is connected to a first end of a tension member. A second end of the tension member is connected to an atraumatic pad. The leader is advanced through the needle from one end of the needle to the other. The leader is further advanced until the second end of the tension member is proximate the heart and the first end of the tension member is external to the heart. A second

atraumatic pad is connected to the first end of the tension member such that the first and second atraumatic pads engage the heart.

Yet another method of placing a heart wall tension apparatus on a heart includes the step of extending a needle having a flexible tension member
5 releasably connected thereto through at least one chamber of the heart such that opposite ends of the tension member are external to the chamber and exposed on opposite sides of the chamber. The needle is removed from the tension member. Then first and second atraumatic pads are connected to the tension member at opposite ends of the tension member.

10 In the treatment of heart failure due to infarcted tissue, possibly including an aneurysm as well, another aspect of the invention involves placing the splint relative to the infarcted or aneurysmal zone, and, in a preferred embodiment, diametrically across the infarcted or aneurysmal zone, to decrease the stress on the infarcted tissue and adjacent border zone tissue. An alternative to diametric
15 placement of the splint includes placing one atraumatic anchor member of the splint at the center of the infarcted or aneurysmal region, extending the splint across the entire heart chamber, and placing the second atraumatic anchor member on the opposite chamber wall. In the case of infarcted or aneurysmal tissue in the vicinity of the mitral valve, an aspect of the present invention
20 includes a method of placing the splint adjacent but below the mitral valve to draw the papillary muscles together or the walls of the valve seat together. It is also envisioned to use the splint both as the sole device for treating infarcted tissue and aneurysms or in combination with the surgical techniques described earlier.

25 An external splint, using a compression member, also may be used to treat a heart having infarcted or aneurysmal tissue. The compression member is placed entirely exterior to the heart and positioned so as to result in similar effects as discussed above with reference to the splint.

Other inventive methods and devices to treat infarcted tissue and
30 aneurysms include a variety of patching and suturing methods and related devices. Each of these methods and related devices reduces the radius of

curvature of the infarcted wall region and adjacent regions and contains the infarcted region to stop further progression.

A further aspect of the invention involves the identification of aneurysmal and infarcted regions using any one or more of a variety of devices and methods.

5 These devices and methods, which will be described more specifically herein, include a bipolar electrode, liquid dye injection and tracing, fiber optics, MRI, and ultrasound. These devices can be used to distinguish between healthy and infarcted heart tissue.

In accordance with the purposes of the invention as embodied and
10 broadly described herein, methods and related devices for treating a heart having infarcted tissue in one of its chambers are disclosed. In a preferred embodiment of the invention, a method for treating a heart having a zone of infarcted tissue in its chamber includes deforming a wall of the chamber that includes the infarcted tissue such that a radius of curvature of the wall is reduced.

15 In another preferred embodiment of the present invention, the method involves providing at least one tension member having two ends and an anchor on each end. The tension member is positioned transverse to the chamber to reduce the radius of curvature of the wall of the chamber that includes the infarcted tissue and/or to draw the walls containing the infarcted tissue together.

20 In another preferred embodiment, the present invention involves positioning a tension member having anchors on each of its ends transverse to the heart chamber so that the infarcted tissue is drawn toward an interior of the heart chamber. The anchors are placed exterior to the chamber.

In yet another preferred embodiment, the present invention includes
25 positioning a compression member having a first end and a second end, each having anchor members around an exterior of the heart. The compression member is positioned so as to surround the chamber with infarcted tissue and to reduce the radius of curvature of the portion of the heart wall that has the infarcted tissue.

30 In accordance with another preferred embodiment, a method of treating a heart having infarcted tissue in one of its chambers involves epicardial suturing

around the perimeter of a region of infarcted tissue and pulling free ends of the suture to draw the infarcted tissue region together. The suture is then secured to hold the infarcted tissue together. This suture also may be employed in combination with a myocardial patch or a substantially rigid enclosure member, both of which represent other preferred embodiments of the present invention.

In accordance with another preferred embodiment of the present invention, a method of treating a heart having infarcted tissue in one of its chambers involves positioning an enclosure member around a zone of infarcted tissue. During the positioning, the enclosure member has a first configuration. After positioning, the enclosure member is then secured to a wall of the heart and the enclosure member reconfigures to a second configuration. Upon reconfiguration to the second configuration, the radius of curvature of the portion of the heart wall including the infarcted tissue reduces.

In accordance with yet another preferred embodiment of the present invention, an apparatus for treating a heart having a zone of infarcted tissue in one of its chambers is provided. The apparatus includes an enclosure member adapted to assume a first configuration during placement of the enclosure member around an infarcted tissue zone. The enclosure member further is adapted to assume a second configuration after securing the enclosure member to a heart wall surrounding the chamber. The second configuration draws the infarcted tissue toward a center of the enclosure member and reduces the radius of curvature of the heart wall.

In accordance with another preferred embodiment of the present invention, a device for treating a heart having infarcted tissue in one of its chambers is provided. The device includes a patch adapted to be attached to the heart, with a substantially elongated member secured to the patch. When the patch is placed over the infarcted or aneurysmal tissue region, the elongated member tends to push the infarcted tissue region toward an interior of the heart chamber.

In accordance with yet another preferred embodiment of the present invention, a plurality of sutures are attached at one end to points on a chamber

wall proximate to an infarcted tissue region and the sutures are extended up through a space defined by an enclosure member to draw the infarcted tissue together and through the enclosure member. The other ends of the sutures are then attached to points on the wall of the chamber to hold the tissue in place.

5 It is to be understood that both the foregoing general description and the following detailed description are exemplary and explanatory only and are not restrictive of the invention, as claimed.

BRIEF DESCRIPTION OF THE DRAWINGS

10 The accompanying drawings, which are incorporated in and constitute a part of this specification, illustrate several embodiments of the invention and, together with the description, serve to explain the principles of the invention. In the drawings,

 Figure 1 is a transverse cross-section of the left and right ventricles of a
15 human heart showing the placement of a splint in accordance with the present invention;

 Figure 2 is a transverse cross-section of the left and right ventricles of a human heart showing the placement of a balloon device in accordance with the present invention;

20 Figure 3 is a transverse cross-section of the left and right ventricles of a human heart showing the placement of an external compression frame structure in accordance with the present invention;

 Figure 4 is a transverse cross-section of the left and right ventricles of a human heart showing a clamp in accordance with the present invention;

25 Figure 5 is a transverse cross-section of the left and right ventricles of a human heart showing a three tension member version of the splint of Figure 1;

 Figure 6 is a transverse cross-section of the left and right ventricles of a human heart showing a two tension member version of the splint shown in Figure 1;

Figure 7 is a vertical cross-sectional view of the left ventricle of a human heart showing an alternate version of the splint in accordance with the present invention;

Figure 8 is an end of the splint shown in Figure 7;

5 Figure 9 is a vertical cross-sectional view of a chamber of a human heart showing another alternative embodiment of the splint in accordance with the present invention;

10 Figure 10 is a vertical cross-section of a chamber of a human heart showing another alternative configuration of splints in accordance with the present invention;

Figure 11 is a vertical cross-sectional view of a chamber of a human heart showing another embodiment of a splint in accordance with the present invention;

15 Figure 12 is a vertical cross-sectional view of a chamber of a human heart showing another embodiment of the splint in accordance with the present invention;

Figure 13 is a vertical cross-sectional view of a chamber of a human heart showing a compression member version of the splint in accordance with the present invention;

20 Figure 14 is a vertical cross-sectional view of a chamber of a human heart showing another version of the splint shown in Figure 13;

Figure 15 is a vertical cross-sectional view of a chamber of a human heart showing a frame member version of the splint in accordance with the present invention;

25 Figure 16 is an end view of the splint of Figure 15;

Figure 17 is a vertical cross-section of the left ventricle and atrium, the left ventricle having aneurysmal scar tissue;

30 Figure 18 is a vertical cross-section of the heart of Figure 17 showing the splint of Figure 1 drawing the aneurysmal scar tissue toward the opposite wall of the left ventricle;

Figure 19 is a vertical cross-section of the left ventricle and atrium of a human heart showing a version of the splint of Figure 1 having an elongate anchor bar;

Figure 20 is a side view of an undeployed hinged anchor member;

5 Figure 21 is a side view of a deployed hinged anchor member of Figure 20;

Figure 22 is a cross-sectional view of a captured ball anchor member;

Figure 23 is a perspective view of a cross bar anchor member;

Figure 24 is a cross sectional view of an alternate anchor pad;

10 Figure 25 is a cross sectional view of an alternate anchor pad;

Figure 26 is a perspective view of yet another alternate embodiment of an anchor pad including an anchor pad loosening device;

Figure 27 is a perspective view of a tension member clip;

15 Figure 28 is a cross sectional view of an alternate embodiment of a tension member clip;

Figure 29 is a cross sectional view of a heart including a tension member having a heat set end;

Figure 30 is a cross sectional view of the pad including an envelope;

Figure 31 shows the envelope of Figure 30;

20 Figure 32 is a side view of a multifilament twisted cable;

Figure 33 is a cross sectional of the cable of Figure 32;

Figure 34 is a side of a multifilament braided tension member;

Figure 35 is a schematic generally horizontal cross sectional view of the heart showing preferred tension member alignments;

25 Figure 36 is a idealized cylindrical model of a left ventricle of a human heart;

Figure 37 is a splinted model of the left ventricle of Figure 36;

Figure 38 is a transverse cross-sectional view of Figure 15 showing various modeling parameters;

30 Figure 39 is a transverse cross-section of the splinted left ventricle of Figure 15 showing a hypothetical force distribution;

Figure 40 is a second transverse cross-sectional view of the model left ventricle of Figure 15 showing a hypothetical force distribution;

Figure 41 is a transverse, partial cross-section of left and right ventricles showing a traditional surgical method of treating infarcted tissue regions;

5 Figure 42 is a transverse, partial cross-sectional view of left and right ventricles with an infarcted or aneurysmal region in the apical portion of the left ventricle and a splint according to an embodiment of the invention placed diametrically across the region;

10 Figures 43a-43b are long axis cross-sectional views of left and right ventricles showing a region of infarcted tissue in a portion of the basal left ventricle and a splint according to an embodiment of the invention placed across the infarcted region;

Figures 43c-43d are short axis cross-sectional views of the heart in Figures 43a-43b shown from the perspective of lines c-c and d-d, respectively;

15 Figures 44a-44b are short axis cross-sectional views of the left ventricle having an aneurysm and a placement of a splint according to an embodiment of the present invention with respect to the aneurysm to treat the heart;

20 Figure 45 is a short axis cross-sectional view of the right and left ventricles having an infarcted region like that shown in Figure 43c and an external splint device according to an embodiment of the present invention placed to treat the infarction;

25 Figures 46a-46c show transverse, partial cross-sectional views of a left ventricle having an infarcted region, illustrating the combined inventive method of surgical removal of the infarcted tissue and placement of a splint according to an embodiment of the present invention;

30 Figure 47 is a short axis cross-sectional view of the left and right ventricles including a view of the mitral valve with an infarcted or aneurysmal region in a portion of the basal left ventricle and a splint according to an embodiment of the invention placed in the vicinity of the mitral valve;

Figures 48a-48b are short axis cross-sectional views of the left and right ventricles and a view of the mitral valve with an aneurysmal region in a portion of the basal left ventricle and an external device according to an embodiment of the invention placed in the vicinity of the mitral valve and aneurysm;

5 Figures 49a-49b are transverse cross-sections of a left ventricle having an aneurysmal region and the placement of a staked patch according to an embodiment of the present invention;

 Figures 50a-50b are planar views of an infarcted or aneurysmal tissue region with a purse-string suture according to an embodiment of the present
10 invention;

 Figures 51a-51c are planar views of an infarcted or aneurysmal tissue region and a purse-string suture and enclosure member according to an embodiment of the present invention;

 Figures 52a-52c are planar exterior views of the heart with an infarcted
15 region of tissue in the left ventricle and an enclosure member according to an embodiment of the invention, showing one configuration during application of the member and a second configuration after application of the member;

 Figure 53a-53b are planar views of an infarcted or aneurysmal tissue region and placement of a tie enclosure according to an embodiment of the
20 present invention;

 Figure 54 is a planar view of yet another embodiment of an enclosure member according to an embodiment of the present invention; and

 Figure 55 is a transverse, partial cross-section of left and right ventricles with an aneurysmal region located at an apical portion of the left ventricle and
25 infarcted tissue along the septal wall.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

 The various aspects of the invention to be discussed herein generally pertain to devices and methods for treating heart conditions, including, for
30 example, dilatation and infarction, including infarction causing aneurysms. For the purposes of providing clarity and consistency throughout the remaining

description of the invention, the following terms have the general definitions set forth below:

"infarction" or "infarcted": refers to myocardium (also described as tissue or muscle) that has lost its ability to contract as a result of cellular necrosis, this term can include, for example, aneurysmal tissue and scar tissue that replaces the necrotic cellular muscle tissue;

"aneurysm" or "aneurysmal": refers to infarcted myocardium that is dyskinetic with respect to surrounding portions of the myocardium;

"contractile": refers to myocardium that is not infarcted and has generally retained contractile potential, though this muscle tissue may not be fully contracting given other conditions, e.g. too much wall stress; and

"border zone": refers to chamber wall that has a region of infarcted tissue and a region of contractile tissue through its thickness.

These definitions are generally consistent with the accepted definitions recognized by those skilled in the art.

The devices of the present invention operate passively in that, once placed in the heart, they do not require an active stimulus either mechanical, electrical, or otherwise, to function. The devices alter the shape or geometry of the heart, both locally and globally, and increase the heart's efficiency by their placement with respect to the heart. That is, the heart experiences an increased pumping efficiency through an alteration in its shape or geometry and concomitant reduction in stress on the heart walls.

The inventive devices and methods offer numerous advantages over the existing treatments for various heart conditions. The devices are relatively easy to manufacture and use, and the related surgical techniques for their implementation do not require the invasive procedures of current surgical techniques. For instance, the surgical technique does not necessarily require

removing portions of the heart tissue, opening the heart chamber, or stopping the heart. For these reasons, the surgical techniques of the present invention are also less risky to the patient than other techniques.

The devices and methods of the present invention used to treat infarcted
5 tissue and aneurysms also are likely to be more effective than prior devices. As
will be described, the inventive devices alter the shape or geometry of the
chamber, either globally or locally, and reduce the radius of curvature of the
chamber wall, resulting in lower stresses in the heart wall. Moreover, with many
of the inventive devices there is no need to open the heart chamber to deploy the
10 device, even when the device is deployed on the septal wall. These methods and
devices also could be used in conjunction with coronary artery bypass grafting
(CABG). In CABG surgery, the use of the inventive methods and related
devices allow for quickly reducing stress on the myocardium, which may save
"stunned" tissue, i.e., tissue that is being starved of nutrients carried with the
15 blood flow, that otherwise may not be recoverable after a certain time period.
Also, the inventive methods and device may hinder further progression or
dilation of scarred, non-contractile tissue.

The disclosed inventive methods and related devices involve geometric
reshaping of the heart. In certain aspects of the inventive methods and related
20 devices, substantially the entire chamber geometry is altered to return the heart
to a more normal configuration. Figures 36 through 40, which will be described
in further detail later, show a model of this geometric reshaping, which includes
a reduction in radius of curvature of the chamber walls. Prior to reshaping the
chamber geometry, the heart walls experience high stress due to a combination
25 of both the relatively large increased diameter of the chamber and the thinning of
the chamber wall. Geometric reshaping according to the present invention
reduces the stress in the walls of the heart chamber to increase the heart's
pumping efficiency, as well as to stop further dilatation of the heart.

Other aspects of the inventive methods and devices involve geometric
30 reshaping a particular area of the chamber and/or reducing the radius of
curvature of the chamber wall in that area. When portions of the heart wall form

a bulge due to an aneurysm, the radius of much of the heart chamber changes. This increases stress on the heart walls. Additionally, the healthy regions of the heart work harder to pump in order to make up pumping volume due to lost contractility in the infarcted tissue region. Together, these effects limit the pumping effectiveness of the heart and can contribute to further degradation of the heart. Geometrically reshaping the area of the aneurysm by, for example, reducing the radius of curvature of the wall, lowers stress on the wall regions in that vicinity and improves pumping function. In addition, the geometric reshaping permits the scar tissue to heal in a more organized fashion and reduces progression of the scar tissue into other areas and further aneurysmal bulging.

Although many of the methods and devices are discussed below in connection with their use in the left ventricle of the heart, these methods and devices may be used in other chambers of the heart for similar purposes. One of ordinary skill in the art would understand that the use of the devices and methods described herein would be substantially the same if employed in other chambers of the heart. The left ventricle has been selected for illustrative purposes because a large number of the disorders that the present invention treats occur in the left ventricle.

Reference will now be made in detail to the present preferred embodiments of the invention, examples of which are illustrated in the accompanying drawings. Wherever possible, the same reference numbers will be used throughout the drawings to refer to the same or like parts.

Figure 1 shows a transverse cross-section of a left ventricle 10 and a right ventricle 12 of a human heart 14. Extending through the left ventricle is a splint 16 including a tension member 18 and oppositely disposed anchors 20. Splint 16, as shown in Figure 1, has been positioned to draw opposite walls of left ventricle 10 toward each other to reduce the "radius" of the left ventricular cross-section or the cross-sectional area thereof to reduce left ventricular wall stresses. It should be understood that although the splint 16 and the alternative devices disclosed herein are described in relation to the left ventricle of a human heart, these devices could also be used to reduce the radius or cross-sectional

area of the other chambers of a human heart in transverse or vertical directions, or at an angle between the transverse and vertical.

Those apparatus of the present invention which reduce heart wall stress by changing chamber wall geometry can be referred to as "splints". "Full cycle
5 splints" engage the heart to produce a chamber shape change throughout the cardiac cycle. "Restrictive splints" do not engage the heart wall at end systole to produce a chamber shape change.

Figure 2 discloses an alternate embodiment of the present invention, wherein a balloon 200 is deployed adjacent the left ventricle. The size and
10 degree of inflation of the balloon can be varied to reduce the radius or cross-sectional area of left ventricle 10 of heart 14.

Figure 3 shows yet another alternative embodiment of the present invention deployed with respect to left ventricle 10 of human heart 14. Here a compression frame structure 300 is engaged with heart 14 at atraumatic anchor
15 pads 310. A compression member 312 having an atraumatic surface 314 presses against a wall of left ventricle 10 to reduce the radius or cross-sectional area thereof.

Figure 4 is a transverse cross-sectional view of human heart 14 showing yet another embodiment of the present invention. In this case a clamp 400
20 having atraumatic anchor pads 410 biased toward each other is shown disposed on a wall of left ventricle 10. Here the radius or cross-sectional area of left ventricle 10 is reduced by clamping off the portion of the wall between pads 410. Pads 410 can be biased toward each other and/or can be held together by a locking device.

Each of the various embodiments of the present invention disclosed in
25 Figures 1-4 can be made from materials which can remain implanted in the human body indefinitely. Such biocompatible materials are well-known to those skilled in the art of clinical medical devices.

Figure 5 shows an alternate embodiment of the splint of Figure 1 referred
30 to in Figure 5 by the numeral 116. The embodiment 116 shown in Figure 5 includes three tension members 118 as opposed to a single tension member 18 as

shown in Figure 1. Figure 6 shows yet another embodiment of the splint 216 having four tension members 218. It is anticipated that in some patients, the disease process of the failing heart may be so advanced that three, four or more tension members may be desirable to reduce the heart wall stresses more substantially than possible with a single tension member as shown in Figure 1.

Figure 7 is a partial vertical cross-section of human heart 14 showing left ventricle 10. In Figure 7, another splint embodiment 316 is shown having a tension member 318 extending through left ventricle 10. On opposite ends of tension member 318 are disposed elongate anchors or pads 320. Figure 8 is an end view of tension member 318 showing elongate anchor 320.

Figure 9 shows another embodiment of a splint 416 disposed in a partial vertical cross-section of human heart 14. Splint 416 includes two elongate anchors or pads 420 similar to those shown in Figures 7 and 8. In Figure 9, however, two tension members 418 extend through left ventricle 10 to interconnect anchors 420 on opposite sides of heart 14.

Figure 10 is a vertical cross section of heart 14 showing left ventricle 10. In this case, two splints 16 are disposed through left ventricle 10 and vertically spaced from each other to resemble the configuration of Figure 9.

Figure 11 is a vertical cross-sectional view of the left ventricle of heart 14. Two alternate embodiment splints 516 are shown extending through left ventricle 10. Each splint 516 includes two tension members 518 interconnecting two anchors or pads 520.

Figure 12 is yet another vertical cross-sectional view of left ventricle 10 of heart 14. An alternate embodiment 616 of the splint is shown extending through left ventricle 10. Splint 616 includes an elongate anchor pad 620 and two shorter anchors or pads 621. Splint 616 includes two tension members 618. Each tension member 618 extends between anchors 620 and respective anchors 621.

Figure 13 is a vertical cross-sectional view of left ventricle 10 of heart 14. A splint 50 is shown disposed on heart 14. Splint 50 includes a compression member 52 shown extending through left ventricle 10. Opposite ends of

compression member 52 are disposed exterior to left ventricle 10. Lever members 54 extend from each end of compression member 52 upwardly along the exterior surface of ventricle 10. A tension member 56 extends between lever

5 members 54 to bias lever members 54 toward heart 14 to compress chamber 10. Compression member 52 should be substantially rigid, but lever members 54 and to some degree compression member 52 should be flexible enough to allow tension member 56 to bias lever members 54 toward heart 14. Alternately, lever members 54 could be hinged to compression member 52 such that lever members 54 could pivot about the hinge when biased toward heart 14 by tension
10 member 56.

Figure 14 shows an alternate embodiment 156 of the splint shown in Figure 13. In this case lever members 154 are longer than members 54 as compression member 152 of splint 150 has been disposed to the exterior of left ventricle 10.

15 Figure 15 is a vertical cross-sectional view of left ventricle 10 of heart 14. An alternate embodiment 250 of the splint is shown on heart 14. A preferably relatively rigid frame member 256 extends through ventricle 10. Disposed on opposite ends of frame 256 are cantilever member 254. Disposed on cantilever members 254 are atraumatic pads 258. Cantilever members 254 can be
20 positioned along frame member 256 such that atraumatic pads 258 press against heart 14 to compress chamber 10. Figure 16 is an end view of frame member 256 showing cantilever members 254 and pads 258.

It should be understood that each of the embodiments described above should be formed from suitable biocompatible materials known to those skilled
25 in the art. The tension members can be formed from flexible or relatively more rigid material. The compression members and frame member should be formed from generally rigid material which may flex under load, but generally hold its shape.

As will be described in more detail herein, Figure 17 is a partial vertical
30 cross-section of human heart 14 showing left ventricle 10 and left atrium 22. As shown in Figure 17, heart 14 includes a region of scar tissue 24 associated with

an aneurysm or ischemia. As shown in Figure 17, the scar tissue 24 increases the radius or cross-sectional area of left ventricle 10 in the region affected by the scar tissue. Such an increase in the radius or cross-sectional area of the left ventricle will result in greater wall stresses on the walls of the left ventricle.

5 Figure 18 is a vertical cross-sectional view of the heart 14 as shown in Figure 17, wherein a splint 16 has been placed to draw the scar tissue 24 toward an opposite wall of left ventricle 10. As a consequence of placing splint 16, the radius or cross-sectional area of the left ventricle affected by the scar tissue 24 is reduced. The reduction of this radius or cross-sectional area results in reduction
10 in the wall stress in the left ventricular wall and thus improves heart pumping efficiency.

 Figure 19 is a vertical cross-sectional view of left ventricle 10 and left atrium 22 of heart 14 in which a splint 16 has been placed. As shown in Figure 19, splint 16 includes an alternative anchor 26. The anchor 20 is preferably an
15 elongate member having a length as shown in Figure 19 substantially greater than its width (not shown). Anchor bar 26 might be used to reduce the radius or cross-sectional area of the left ventricle in an instance where there is generalized enlargement of left ventricle 10 such as in idiopathic dilated cardiomyopathy. In such an instance, bar anchor 26 can distribute forces more widely than anchor
20 20.

 Figures 20 and 21 are side views of a hinged anchor 28 which could be substituted for anchors 20 in undeployed and deployed positions respectively. Anchor 28 as shown in Figure 20 includes two legs similar to bar anchor 26. Hinged anchor 28 could include additional legs and the length of those legs
25 could be varied to distribute the force over the surface of the heart wall. In addition there could be webbing between each of the legs to give anchor 28 an umbrella-like appearance. Preferably the webbing would be disposed on the surface of the legs which would be in contact with the heart wall.

 Figure 22 is a cross-sectional view of a capture ball anchor 30. Capture
30 ball anchor 30 can be used in place of anchor 20. Capture ball anchor 30 includes a disk portion 32 to distribute the force of the anchor on the heart wall,

and a recess 34 for receiving a ball 36 affixed to an end of tension member 18. Disk 32 and recess 34 include a side groove which allows tension member 38 to be passed from an outside edge of disk 32 into recess 34. Ball 36 can then be advanced into recess 34 by drawing tension member 18 through an opening 38
5 in recess 34 opposite disk 32.

Figure 23 is a perspective view of a cross bar anchor 40. The cross bar anchor 40 can be used in place of anchors 20. The anchor 40 preferably includes a disk or pad portion 42 having a cross bar 44 extending over an opening 46 in pad 42. Tension member 18 can be extended through opening 46 and tied to
10 cross bar 42 as shown.

Figure 24 is a cross sectional view of an alternate embodiment of anchor pad 340 in accordance with the present invention. Anchor pad 340 preferably includes a disc shaped pad portion 342. Disc-shaped pad portion 342 includes side 343, which in use is disposed toward the heart. A conical aperture 348
15 having sloping sides 346 extends through pad 342. Collet 344 is disposed within orifice 348. A threaded portion 350 of collet 344 extends from orifice 348 opposite side 343, nut 352 is threaded over threaded portion 350. Lumen 345 extends through collet 344. A tension member 354 is shown extending through lumen 345. Lumen 345 has a diameter such that when nut 352 is not tightened
20 on threaded portion 350, tension member 354 can slide freely through lumen 345. When nut 352 is tightened, it draws collet 344 away from side 343. Collet 344 is then pinched between walls 346 of orifice 348. When collet 344 is pinched, the size of lumen 345 is reduced such that tension member 354 can no longer move freely within lumen 345, fixing the position of pad 340 on tension
25 member 354.

Figure 25 is a cross sectional view of an alternate embodiment of an anchor pad 360 in accordance with the present invention. Anchor pad 360 includes a generally disc-shaped pad portion 362. Pad 362 includes a side 363 which when the pad is in use, is disposed toward the heart. A tension member
30 lumen 364 extends through pad 362. Lumen 364 preferably has a generally conical shaped portion 365 disposed toward side 363. Tension member 370 is

shown disposed through lumen 364 in Figure 25. Pad 362 includes a threaded passage 366 extending from an edge of pad 362 to lumen 364. A set screw 368 is threaded into passage 366. Set screw 368 can be tightened to engage tension member 370 to fix the position of anchor pad 360. When set screw 368 is not tightened, the size of lumen 364 is preferably large enough that anchor pad 360 can slide relatively freely over tension member 370.

Figure 26 is a perspective view of yet another embodiment of anchor pad 380 in accordance with the present invention. Anchor pad 380 preferably includes a generally disc-shaped pad portion 382 having a first side 383 which in use would be disposed toward the heart and a second side 385. Pad 382 as well as pads 342 and 362 are preferably formed from a metal such as stainless steel alloys or titanium alloys.

A tension member fastener 384 is formed in pad 382 by cutting a series of grooves and apertures through pad 382 from side 385 to side 383. A first groove 386 has a generally horseshoe shape. Second groove 388 extends between opposite portions of horseshoe shaped groove 386 to form two oppositely disposed cantilever members 387. A relatively large aperture 394 is formed between cantilever members 387 proximate their free ends. A second and smaller aperture 390 is formed closer to the fixed ends of cantilever members 387. Tension member 392 is shown extending through aperture 390.

As shown in Figure 26, tension member 392 is clamped between cantilever members 387 such that the location of pad 382 is fixed along tension member 392. Pad 382 can be released by using a spreading device 396 to spread cantilever members 387 apart. Spreading device 396 includes handle 398 to spreading arms 400 each having a finger 402. Fingers 402 can be placed within aperture 394 then arms 400 and fingers 402 can be spread apart by pivoting them around a pin 404 such that cantilevers 387 are spread apart and pad 382 can move freely along tension member 392. It can be appreciated that although spreader 396 is shown extending transversely from tension member 392, it could also be configured such that fingers 402 do not curve transversely from arms 400 and thus spreader 396 could be disposed parallel to tension member 392. This

would be particularly desirable in a situation where anchor pad 380 was being placed through a port or window during a less invasive splint implantation procedure. It can be appreciated that cantilever members 387 can be held apart such that pad 380 can be moved along tension member 392 by placement of a temporary wedge or pin in groove 388. For example, grooves 388 may include an additional small aperture disposed between aperture 390 and aperture 394 into which a pin could be placed to hold open members 387. When it is desired to fix the position of anchor pad 380 on tension member 392, device 396 could be used to spread cantilever members 387 to remove the pin. The cantilever members could then be released to engage tension member 392. Aperture 390 of pad 380 can also include a conical portion disposed toward side 383 such as conical portion 365 of pad 360.

Cantilever arms 384 are preferably configured such that they do not stress tension member 392 beyond its elastic limit. It can also be appreciated that the force developed by cantilever members 387 impinging on tension member 392 is operator independent and defined by the geometry and material characteristics of members 387.

Figure 27 is a perspective view of an anchor pad 360 having a tension member 370 extending therethrough. After pad 360 is secured to tension member 370, that portion of tension member 370 which extends from the side of anchor pad 360 opposite side 363 is preferably removed. This can be accomplished by trimming tension member 370 with wire cutter 414 or scissors. Although anchor pad 360 is used here to illustrate trimming tension member 370, it can be appreciated that in each of the embodiments disclosed herein there may be an excess portion of tension member extending from an anchor, which is preferably removed or trimmed.

Figure 28 is a cross sectional view of an alternate embodiment 420 of a tension member cutter. Device 420 includes an elongate outer tube 422 having a distal end 424. Tube 424 defines a lumen 423 through which extends a second tube 430 having a distal end 428. Extending distally from distal end 428 are two cutting arms 424 and 426 which are shown partially withdrawn into lumen 423

and transversely restrained by distal end 424 of outer tube 422. When unrestrained by distal end 424, arms 424 and 426 are biased apart. Each arm 424 and 426 has a cutting element 425 and 427, respectively. Elements 425 and 427 are shown in contact with each other in Figure 28. A tension member 370
5 extends between arms 424 and through lumen 432 of inner tube 430. A representative anchor pad 360 is disposed adjacent elements 425 and 427. Device 420 of Figure 28 is particularly useful when trimming excess tension member using less invasive techniques as it can be readily advanced over a tension member through a port or window trocar.

10 Figure 29 is a vertical cross sectional view of left ventricle B of heart A. A transventricular splint 443 including a tension member 370 and anchor pads 360 are shown disposed on heart A. To the left of heart A as shown in the figure is a coiled portion 442 of tension member 470. As an alternative to trimming an excess length of tension member, tension member 370 could be formed from a
15 shape memory alloy such that portion 442 could be preset to assume a coil shape when warmed to near body temperature.

Once the length of the tension member has been adjusted, the anchors are secured in place along the tension member and the excess length of tension member removed if desired, the anchor or anchor pads are preferably secured in
20 place on the heart. The anchor or anchor pads are secured such that relatively movement between the anchors or anchor pads and the heart is limited to reduce abrasion of the heart wall. To secure the anchor or anchor pads to heart A, a biocompatible adhesive could be placed between the pad and the heart to adhere the pad to the heart. Alternately, apertures could be provided in the pad such
25 that sutures could be extended through the apertures and into the heart to secure the pad. In addition to sutures, the pad could include threaded apertures into which anchor screws could be advanced through the pad and into the heart wall to secure the pad to the heart.

Figure 30 illustrates yet another alternative approach to securing the
30 anchors or anchor pads to the heart surface. Figure 30 is a cross sectional view of an anchor pad 340 disposed on heart A. Anchor pad 340 is disposed within

an envelope 446. Envelope 446 includes a bottom layer 447 disposed between anchor pad 340 and heart A and a top layer 448 disposed on the opposite side of anchor pad 340. Layers 347 and 340 are held together by sutures 449. Bottom layer 447 is preferably a mesh or expanded PTFE which has a pore size or
5 intranodial dimension sufficient to promote tissue ingrowth. The pore size is preferably between about 10 and about 100 microns and more preferably, between about 20 and about 40 microns. With respect to expanded PTFE, the intranodial dimension is preferably between about 10 to about 100 microns and more preferably between about 20 to about 40 microns. The top material could
10 also be expanded PTFE or the like having a pore size which preferably does not promote ingrowth and thus resists adhesion to surrounding tissue. As an alternative embodiment, the pores could be formed directly in the pad surface.

Envelope 446 would preferably be placed around pad 340 prior to placing pad 340 on tension member 354. A window 450 can be provided to provide
15 access to nut 352 to secure pads to tension member 354. After tightening nut 352, window 450 can be closed by suture 452. Figure 31 is a top view of pad 340 and envelope 446 of Figure 30. It can be appreciated that a similar envelope can be placed around the various anchor pads disclosed herein. The location of the window may have to vary, however, to provide access to the respective
20 means for securing the anchor pads to the tension member.

The splints of the present invention can be implanted acutely or chronically. When the splints are implanted chronically, it is particularly important that the tension member or members be highly fatigue resistant. Typical materials for the tension member can include, among other
25 biocompatible materials, stainless steel, titanium alloys, NiTi alloys such as Nitinol or elgiloy. In a preferred embodiment, the tension member is a wire having a diameter of between 0.005 to 0.035 inches in diameter or, more preferably, between 0.01 and 0.02 inches in diameter and, most preferably, about 0.014 inches in diameter. The length of the tension member between the pads is
30 preferably about 0.6 to 4 inches, and more preferably, between about 1 to 3 inches and, most preferably, about 2 inches. To improve the fatigue resistance

of the metallic tension members, their surface can be electro-polished, buffed or shot peened. Drawing or annealing of the metal will also improve fatigue resistance.

The tension member, in a preferred embodiment, articulates with respect to the anchor pad to reduce bending of the tension member at the pad. This can be accomplished by a ball and socket joint shown in Figure 22, for example. The tension member itself can be made more flexible or bendable by providing a multi-filament tension member such as a braided or twisted wire cable tension member. A multifiber filament structure of numerous smaller wires can then easily, while reducing the stress level on any individual wire as compared to a solid wire of the same diameter as the multifilament bundle. Such a multi-filament tension member can be made from biocompatible materials such as, but not limited to, stainless steel, Nitinol, titanium alloys, LCP (liquid crystal polymer), SpectraJ fiber, kevlar fiber, or carbon fiber. In a preferred embodiment, the multi-filament structure is coated or covered to substantially seal the multi-filament structure. Coatings such as silicone, urethane or PTFE are preferred.

Figure 32 is a side view of multifilament twisted cable 400. Cable 400 includes a plurality of wires or filaments 402 twisted about the longitudinal axis of cable 400. Figure 33 is a transverse cross sectional view of cable 400. In Figure 33, cable 400 includes a surrounding coating 404 not shown in Figure 32.

Figure 34 is a side view of a braided multifilament tension member 410. Tension member 410 includes a plurality of filaments or wires 412. It can be appreciated that numerous braiding patterns are known to those skilled in the art of multifilament members. It is anticipated that in a preferred embodiment, braided member 410 can have an optional core of fibers running parallel to an elongate axis of tension member 410. In yet another preferred embodiment, tension member 410 could have a solid wire core extending parallel to and along the longitudinal axis of tension member 410.

The tension members and anchors or anchor pads are preferably bio-resistant, i.e., resistant to physiologic attack. To improve bio-resistance, tension member and/or anchors or anchor pads can be coated with carbon material such as glass, pyrolytic carbon, diamond or graphite, zirconium nitrate or oxide. Roughened or porous urethanes, silicone or polymer coatings or sheaths can be used to promote tissue ingrowth to create a biological seal. Hydrophilic and albumin coatings can also be used. Drugs incorporated into a binder coating can also be used to reduce biological attack on the splint and irritation of tissue by the splint. Such drugs include heparin, coumadin, anti-inflammatory steroid or ASA-aspirin. The oxide layer of the underlying metal could also be optimized to improve bio-resistance. This is particularly true for stainless steel, titanium, or nickel titanium on which an oxide layer can be formed by heating the component to improve biocompatibility. Further coatings include calcium hydroxy appetite, beta tricalcium phosphate and aluminum oxide can be applied to the tension member. The tension member and/or pad or anchor pad can at least be, in part, formed from titanium to enhance electronegativity.

The anchors or anchor pads and, particularly the tension members are biocompatible, preferably antithrombogenic and made to prevent hemolysis. The coatings used to enhance bio-resistance described above can generally be used to improve biocompatibility. Since the tension member is exposed to significant blood flows through the left ventricle, in a preferred embodiment, the tension member has a generally small size and shape elliptical cross sectional shape to reduce turbulence or drag over the tension member. If such elliptical, transverse cross section tension member were used, it can be appreciated that the narrow end would be preferably oriented toward the direction of blood flow. It is also desirable to select a tension member material and shape which would not vibrate at resonant frequency under the influence of blood flow.

Where the tension member passes through the heart wall, various approaches can be taken to reduce or prevent bleeding. For example, the surface of the anchor or anchor pad and/or tension member in contact with the heart wall

can be coated or include an ingrowth inducing covering such as collagen, dacron, expanded PTFE or a roughened/porous surface. A clotting inducing substance may also be bound to the tension member and/or anchor or anchor pads, such as avitene or collagen. It is also contemplated that the portion of the heart wall where the tension member passes through could be cauterized. In a preferred embodiment, the tissue can be cauterized by heating the tension member. A glue such as cyanoacrylate can also be disposed between the tension member and the heart wall to reduce or prevent bleeding from the heart wall. Mechanical means such as an O-ring or compression fitting could also be disposed between the heart wall and the tension member to reduce bleeding. A purse string suture can be placed on the heart, around the tension member adjacent the pad as well.

The tension member is preferably flexible enough to allow for changing interface conditions between the heart and the splint, and alternating pad orientation throughout the cardiac cycle. The flexibility should be sufficient enough to avoid injury to the heart or bleeding. It is also preferable that if the heart were to contract sufficiently enough to put the tension member in compression that it would readily buckle. Buckling could be promoted by providing a ribbon shaped tension member, chain link tension member, thin wire tension member, bent tension member or multi-filament tension member.

The tension member is preferably radiopaque, echo cardiographic visible, or MRI compatible or includes a marker which is radiopaque, echo visible, or MRI compatible. The preferred locations for markers would include the center of the tension member and at the ends of the tension member disposed at the heart walls. The radiopaque markers could be gold or platinum or other biocompatible metal or heavy metal filled polymeric sleeves. With respect to echo compatible or MRI compatible tension members or markers, the tension or marker are preferably non-interfering or visible. Having radiopaque echo compatible or MRI compatible tension members or markers is particularly desirable for follow-up, non-invasive monitoring of the tension member after implantation. The presence of the tension member can be visualized and the

distance between two or more markers measured. Integrity of the tension member can be confirmed as well.

In a preferred embodiment, the tension member is not conductive to the action potential of muscle. This can be accomplished by insulating the tension member, anchor and/or anchor pad interface or fabricating the tension member anchor and/or anchor pad from a non-conductive metal such as titanium.

In addition to monitoring the performance of the tension member by visualization techniques such as fluoroscopy or echo imagery, sensors can advantageously be incorporated into the splints. For example, a strain gauge can be disposed on a tension member to monitor the loading on the member in use. Strain can be related to load as known to those skilled in the art by developing a stress/strain relationship for a given tension member. The strain gauge can be connected by a biocompatible lead to a conventional monitoring device. A pressure gauge formed from, for example, piezo electric material can also be disposed on the tension member to monitor filling pressures or muscle contractility.

In a preferred embodiment, a tension member can be slidably enclosed within a tube. If the tension member were to fail, the tube would contain the tension member therein.

It is anticipated that the tension member could be connected to a pacing lead. In such an instance, if the tension member were conductive, pacing signals could be conveyed along the tension member from one heart wall to another.

In use, the various embodiments of the present invention are placed in or adjacent the human heart to reduce the radius or cross-section area of at least one chamber of the heart. This is done to reduce wall stress or tension in the heart or chamber wall to slow, stop or reverse failure of the heart. In the case of the splint 16 shown in Figure 1, a cannula can be used to pierce both walls of the heart and one end of the splint can be advanced through the cannula from one side of the heart to the opposite side where an anchor can be affixed or deployed. Likewise, an anchor is affixed or deployed at the opposite end of splint 16. Additional methods for splint placement are described in more detail in U.S.

Patent Application Serial No. 09/123,977, filed on July 29, 1998 and entitled "Transventricular Implant Tools and Devices" and incorporated herein by reference.

It can be appreciated that the methods described above to advance the
5 tension members through the ventricles can be repeated to advance the desired
number of tension members through the ventricle for a particular configuration.
The length of the tension members can be determined based upon the size and
condition of the patient's heart. It should also be noted that although the left
ventricle has been referred to here for illustrative purposes, that the apparatus
10 and methods of this invention can also be used to splint multiple chambers of a
patient's heart as well as the right ventricle or either atrium.

Figure 35 is a schematic view of generally horizontal cross section of
heart A including left ventricle B and right ventricle C. Also shown are left
anterior descending artery E, posterior descending artery F, obtuse marginal
15 artery G, postero-medial papillary muscle H and antero-lateral papillary muscle
I. Shown in Figure 35 are three generally horizontal preferred alignments for
tension member placement for the splints of the present invention when used for
the purpose of treating ventricular dilatation. These alignments generally met
three goals of splint positioning including good bisection of the left ventricle,
20 avoidance of major coronary vessels and avoidance of valve apparatus including
chordae leaflets and papillary muscles. Alignment 420 can be referred to as the
anterior/posterior (AP) position. Alignment 422 can be referred as the posterior
septal/lateral wall (PSL) position. Alignment 424 can be referred to as the
anterior septal/lateral wall (ASL) position.

25 It can be appreciated that the alignments shown are illustrative only and
that the alignments may be shifted or rotated about a vertical axis generally
disposed through the left ventricle and still avoid the major coronary vessels and
papillary muscles. When the alignment passes through a substantial portion of
right ventricle C, it may be desirable to dispose not only two pads on the exterior
30 of the heart at opposite ends of a tension member, but also a third pad within
right ventricle C on septal J. The spacing between the third pad and the pad

disposed outside the heart proximate left ventricle B preferably defines the shape change of left ventricle B. This will allow the spacing of the third pad relative to the pad disposed outside the heart proximate right ventricle C to define a shape change if any of right ventricle C in view of the spacing between those pads.

5 With the alignments as shown in Figure 35, the third pad will be unnecessary. It is likely, however, that with alignments 422 and 424 in order to achieve the desired shape change of left ventricle B, the exterior pad of the wall proximate the right ventricle C will be drawn into contact with septal J. This will consequently somewhat reduce the volume of right ventricle C.

10 Figure 36 is a view of a cylinder or idealized heart chamber 48 which is used to illustrate the reduction of wall stress in a heart chamber as a result of deployment of the splint in accordance with the present invention. The model used herein and the calculations related to this model are intended merely to illustrate the mechanism by which wall stress is reduced in the heart chamber.

15 No effort is made herein to quantify the actual reduction which would be realized in any particular in vivo application.

Figure 37 is a view of the idealized heart chamber 48 of Figure 36 wherein the chamber has been splinted along its length L such that a "figure eight" cross-section has been formed along the length thereof. It should be noted

20 that the perimeter of the circular transverse cross-section of the chamber in Figure 36 is equal to the perimeter of the figure eight transverse cross-section of Figure 37. For purposes of this model, opposite lobes of the figure in cross-section are assumed to be mirror images.

Figure 38 shows various parameters of the Figure 1 cross-section of the splinted idealized heart chamber of Figure 37. Where l is the length of the splint

25 between opposite walls of the chamber, R_2 is the radius of each lobe, θ is the angle between the two radii of one lobe which extends to opposite ends of the portion of the splint within chamber 48 and h is the height of the triangle formed by the two radii and the portion of the splint within the chamber 48 (R_1 is the

30

radius of the cylinder of Figure 36). These various parameters are related as follows:

$$h = R_2 \cos (\theta/2)$$

$$l = 2 R_2 \sin (\theta/2)$$

5 $R_2 = R_1 \pi / (2\pi - \theta)$

From these relationships, the area of the figure eight cross-section can be calculated by:

$$A_2 = 2\pi(R_2)^2 (1-\theta/2\pi) + hl$$

Where chamber 48 is unsplinted as shown in Figure 36 A_1 the original
10 cross-sectional area of the cylinder is equal to A_2 where $\theta = 180^\circ$, $h = 0$ and $l = 2R_2$. Volume equals A_2 times length L and circumferential wall tension equals pressure within the chamber times R_2 times the length L of the chamber.

Thus, for example, with an original cylindrical radius of four centimeters and a pressure within the chamber of 140 mm of mercury, the wall tension T in
15 the walls of the cylinder is 104.4 newtons. When a 3.84 cm splint is placed as shown in Figures 37 and 38 such that $l = 3.84$ cm, the wall tension T is 77.33 newtons.

Figures 39 and 40 show a hypothetical distribution of wall tension T and pressure P for the figure eight cross-section. As θ goes from 180° to 0° , tension
20 T_s , in the splint goes from 0 to a $2T$ load where the chamber walls carry a T load.

In yet another example, assuming that the chamber length L is a constant 10 cm, the original radius R_1 , is 4 cm, at a 140 mmHg the tension in the walls is 74.7 N. If a 4.5 cm splint is placed such that $l = 4.5$ cm, the wall tension will then be 52.8 N.

25 When a splint is actually placed on the heart, along an alignment such as those shown in Figure 35, the length l between the two pads as measured along the tension member is preferably 0.4 to about 0.8 and more preferably between about 0.5 to about 0.7 and most preferably about 0.6 times the distance along the length of the tension member at end diastole if the pads were not secured to the
30 tension member and provided no resistance to expansion of the heart. A more detailed discussion of tension member length can be found in U.S. Patent

Application Serial No. 09/123,977, filed on July 29, 1998 and entitled "Transventricular Implant Tools and Devices" which is incorporated herein by reference.

As mentioned earlier, Figure 17 is a partial vertical cross-section of human heart 14 showing left ventricle 10 and left atrium 22. As shown in Figure 17, heart 14 includes a region of scar tissue 24 associated with an aneurysm. The aneurysmal scar tissue 24 increases the radius or cross-sectional area of left ventricle 10 in the region affected by the scar tissue. Such an increase in the radius or cross-sectional area of the left ventricle will result in greater wall stresses on the walls of the left ventricle, especially those walls adjacent to the aneurysm.

In addition to the various uses of the splint to treat ventricular dilatation as heretofore discussed, the inventive splint also can be used to treat infarcted tissue or aneurysms occurring on the heart wall, as illustrated by Figures 18 and 42-44, 46, and 47. These figures show various placements of a splint to treat infarcted tissue or aneurysms. It is to be understood that variations of these placements that have similar effects are within the scope of this invention.

Figure 42 illustrates a method for placing a splint of the present invention to treat a heart with infarcted tissue, including an aneurysm. The particular aneurysm A shown in Figure 42 affects the ventricular septal wall. Figure 42 shows a partial transverse cross-section of a human heart having an aneurysm A (shown by shading) in the left ventricle wall. It is contemplated that the methods and devices of this invention also apply to treatment of hearts with akinetic scar tissue that has not progressed past an infarcted stage and into an aneurysmal stage, in which case there would be little or no bulging of the heart wall. Such a condition is shown in Figures 43a-43d to be described shortly. In Figure 42, splint 16 is placed diametrically across aneurysm A to lessen the load carried by the transmural infarcted tissue 24 forming aneurysm A, as well as any adjacent border zone tissue that may be present. The border zone (although not shown in Figure 42) is the portion of the heart wall which has a mix of contractile tissue 24" and infarcted tissue 24. Anchors 20 of splint 16 are located on the outside of

the chamber walls and are placed generally adjacent to the portions of the chamber wall that transition from infarcted myocardium 24 to regions of contractile myocardium 24". Tension member 18 extends through the heart chamber with each of its ends connecting to opposing anchors 20. Anchors 20, especially when used to anchor splint 16 on septal wall S, can be of the self-deploying type disclosed in co-pending application U.S. Serial No. 09/123,977, filed July 29, 1998, entitled "Transventricular Implant Tools and Devices," the complete disclosure of which is incorporated herein by reference.

Splint 16 reduces the radius of curvature of the aneurysmal region A and the adjacent regions of the chamber wall. By reducing the radius of curvature in these regions, contractile regions 24" of the myocardium that were under high stress due to geometric abnormalities associated with an aneurysmal region A are relieved from that high stress, thereby resulting in increased pumping ability upon contraction. Even if the infarcted tissue has not led to bulging of the heart wall, reducing the radius of curvature helps to reduce some of the stress in the adjacent contractile myocardium. By increasing the pumping ability of the contractile myocardium 24", the heart can more easily pump the required blood flow output, helping to offset the pumping lost by the infarcted muscle 24. Those regions of the chamber wall that have only endocardial infarcted tissue, that is border zone regions 24', likely will experience an increase in their ability to contract and contribute to pumping.

It is also contemplated to use more than one splint, and splints having different lengths, to optimize the reduction in the radius of curvature of infarcted and aneurysmal regions and adjacent regions. Another contemplated mode of the invention includes closing off the infarcted or aneurysmal region completely by shortening the splint so that the walls adjacent the anchors contact each other. Closing off the infarcted or aneurysmal tissue from the rest of the heart chamber in this way renders this tissue completely non-functional with respect to contributing to the pumping. Shortening the splint to achieve contact of the heart walls may also reduce the risk of embolic thrombus because no blood would be expected to flow into the excluded region. Additionally, the need to

remove any thrombus already adhered to the heart wall may be unnecessary because the thrombus would have no way of escaping back into the heart chamber to cause stroke or other malfunctions. If the infarcted or aneurysmal tissue extends to the septal wall of the chamber, the splint would be placed
5 across the chamber so as to exclude the non-contractile tissue of the septal wall as well.

As described earlier, Figure 18 is a vertical cross-sectional view of heart 14 as shown in Figure 17. Figure 18 depicts another method of the present invention, wherein splint 16 is placed to draw aneurysm A toward an opposite
10 wall of left ventricle 10. An anchor 20 of splint 16 is placed on the outside wall of heart 14, approximately at the center of the infarcted tissue 24 forming aneurysm A. Tension member 18, connected to this anchor, is then extended across the chamber of the heart to the opposite wall and connected to another anchor 20 placed on the outside chamber wall to secure splint 16. The radius or
15 cross-sectional area of the left ventricle affected by the infarcted tissue 24 is thereby reduced. The reduction of this radius or cross-sectional area results in reduction in the stress in the left ventricular wall and thus improves heart pumping efficiency. Furthermore, infarcted tissue 24 is supported by anchor 20 of the splint to prevent any additional bulging of the wall or progression of the
20 infarcted tissue to other areas of the myocardium.

Bringing infarcted tissue 24 into the chamber, as shown in Figure 18, likely reduces the risk of thrombosis due to contact between the endocardial infarcted tissue and circulating blood flow occurring in these regions of the chamber. Clots are less likely to form on tissue that is subject to an active flow
25 of blood. The forces associated with such flow diminish stagnation points that allow clots to form and adhere to the wall more readily.

Figures 43a-43d depict the use of splint 16 to treat a heart chamber having a discrete zone of akinetic infarcted myocardium 24 that has not yet developed into an aneurysm. Figures 43a and 43b depict a long axis (or
30 essentially vertical) cross-sectional view of the heart, with Figure 43b showing the placement of splint 16. Figures 43c and 43d show the heart in short axis (or

essentially horizontal) cross-section, with placement of splint 16 shown in Figure 43d. In Figures 43b and 43d, splint 16 is shown treating a heart including infarcted tissue 24 that does not affect septal wall S. Thus, both anchors 20 are placed on exterior wall portions of left ventricle LV. However, it is
5 contemplated that a splint could be used to alter the geometry of the chamber in cases in which an infarcted region does affect septal wall S.

By utilizing splint 16, the radius of curvature, particularly with respect to the short axis direction, is reduced. This reduction of curvature facilitates the pumping ability of any portions near the infarcted region 24 that have some
10 contractile potential by reducing wall stress in the region. By allowing this once marginally contractile tissue to increase its contractile ability, the heart improves its ejection fraction, cardiac reserve, and muscle contractibility. Additionally, the remainder of the ventricle also experiences a reduced radius of curvature, as shown in Figure 43b and 43d, further facilitating the contractile ability of the
15 entire ventricle. By improving the contracting ability of the entire chamber, the heart has the ability to account for the lost pumping ability of the infarcted myocardium 24. Left untreated, this condition causes the rest of the ventricle to attempt to contract more, ultimately over-working and weakening the heart to a greater degree.

20 Figures 44a-44b show a cross-sectional view of the left ventricle with an aneurysmal region A. As shown in Figure 44b, splint 16 can also be placed such that one anchor 20 engages approximately the center of the bulge formed by aneurysm A. Tension member 18 is then extended through the center of aneurysm A and across left ventricle LV to anchor splint 16 to a point on the
25 surrounding heart wall substantially opposite to aneurysm A. This positioning of splint 16 tends to bring the aneurysmal bulge in line with the normal curvature of the heart wall. By this placement of splint 16, it is expected that greater blood flow would occur in the region of aneurysmal tissue A, potentially reducing thrombus formation.

30 Figure 45 shows the use of a completely external device to treat a heart having a zone of infarcted tissue 24. In the embodiment shown in Figure 45, the

external splint device is an external frame generally in the form of a clamp 17 with anchor pads 21 on each end of the clamp. The clamp 17 is configured to exert a compressive force on the heart wall to cause shape change of the heart chamber. Other external splint devices, in addition to clamp 17, that are
5 contemplated for use in treating a heart having infarcted myocardium are disclosed in co-pending U.S. Patent Application Serial No. 09/157,486, filed September 21, 1998, and entitled "External Stress Reduction Device and Method," the complete disclosure of which is incorporated herein by reference. In addition to the benefits described above with respect to using a splint to treat a
10 heart having infarcted tissue, external splint devices such as that shown in Figure 45 include the potential further advantage of significantly reducing the possibility of thrombus formation resulting from surfaces of devices that contact blood flowing through the chamber.

Another use for splint 16 in treating heart chambers having infarcted or
15 aneurysmal tissue is shown with reference to Figures 46a through 46c. This method combines the use of splint 16 with the traditional surgical technique in which the infarcted tissue is removed. By using the techniques described later for identifying and distinguishing between healthy tissue and infarcted tissue, all of the infarcted myocardium 24 shown in Figure 46a can be excised from the
20 chamber, as shown in Figure 46b. The separated portions of the chamber walls will then be sutured back together. Splint 16 is then placed diametrically transverse to the portion of heart chamber walls 24" that have been partially excised, as shown in Figure 46c. Anchors 20 are placed between the portions of the chamber wall from which infarcted tissue 24 was removed and portions of
25 the chamber wall that contained contractile tissue throughout its thickness. Because only contractile tissue regions 24" would remain after this procedure, as opposed to conventional surgery which leaves some of the infarcted tissue occurring in border zone regions in place, contractile function, and thus cardiac function, likely would improve. Splint 16 reduces the radius of curvature in
30 those thinner regions of the walls that remain after the surgery, allowing them to produce stronger contractions and relieving stress in those wall portions.

If the infarcted tissue is not removed, as shown in Figure 42, the border zone cannot contribute significantly to the pumping function, for the contractile muscle must contract against the stiffness of the infarcted muscle. But, with the infarcted tissue removed, the thin contractile section of myocardium shown in
5 Figure 46c can be made to contract and contribute to pumping, particularly since splint 16 has reduced stress enough to allow the thin region of tissue to exert the required pressure to pump. In addition to combining the surgical excision of the infarcted tissue with the use of a splint of the present invention, an external device, like clamp 17 shown in Figure 45, can also be combined with the
10 surgical technique. Such an external device would be placed with respect to the heart chamber walls such that its anchors are disposed in the approximate locations as anchors 20 on splint 16, and the device between the anchors could extend around the portions of the walls that have been sutured together. It is contemplated that the splint 16 could be used in hearts where the aneurysm
15 involves the septal wall of the ventricle. Similar to the splinting shown in Figure 42, one or both anchor pads could be self-deploying.

Another use of the splint to treat infarcted or aneurysmal tissue near the base of a mitral valve MV is shown in Figure 47. In this embodiment, the splint is placed such that its anchors 20 are diametrically opposed to one another across
20 an aneurysm, or generally dilated annular region, located in a portion of the basal left ventricle in the vicinity of mitral valve MV. Anchors 20 are placed on the outer wall of left ventricle LV with tension member 18 of splint 16 drawn through the heart chamber and diametrically across the infarcted or aneurysmal region. The dotted line of tension member 18 shown in Figure 47 illustrates that
25 splint 16 lies below mitral valve MV. Placing the splint in this manner results in the papillary muscles P of mitral valve MV or the leaflets of mitral valve MV being drawn together and reduces the risk of mitral regurgitation. In addition, splint 16 reduces the radius of curvature of the aneurysmal or infarcted region. As previously described, this reduction lowers the stress in the heart wall,
30 improving pumping effectiveness. Figure 47 shows the placement of splint 16 such that both anchors are disposed on external walls of the left ventricle. It

should be noted that the splint also could be placed so that one anchor is disposed on septal wall S, in which case a self-deploying anchor preferably would be used. Also, tension member 16 may be made to curve between anchors 20 in order to avoid damaging internal structures of the ventricle.

5 Figures 48a-48b show the use of an external splint device to treat a heart having an aneurysm A in the vicinity of mitral valve MV. As a result of the aneurysm, the anterior leaflet AL and posterior leaflet PL of mitral valve MV have separated causing mitral regurgitation, as shown in Figure 48a. Figure 48b shows the placement of an external splint device having a clamp portion 19
10 connecting two anchors 25. It is contemplated that the external splint device used to treat this particular heart condition may also include a protrusion 19' as part of clamp portion 19. In placing clamp 19 on the heart, protrusion 19' engages aneurysm A so as to push aneurysm A toward a center of the ventricle. Additionally, a stabilizing bar 23 could be attached to the end of protrusion 19'.
15 Stabilizing bar 23 is configured to extend through the heart chamber wall and anchor to the edge of posterior leaflet PL of mitral valve MV to bring the leaflet in close proximity to anterior leaflet AL. Such a stabilizing bar may be made of a semi-rigid, or rigid, material such as implantable metals or other suitable material. While Figures 48 and 49 show the use of various splints associated
20 with an aneurysm in the vicinity of the mitral valve, it is contemplated to utilize splints also in the case where there is no true aneurysm, but an area of infarcted tissue near the mitral valve.

 The present invention also includes myocardial patches and related methods used to treat aneurysms. Figures 49a-49b illustrate one preferred
25 embodiment of the invention. Figure 49a shows left ventricle LV with an aneurysm A in a portion of the chamber wall. Figure 49b illustrates placement of a staked patch 72 according to an embodiment of the present invention used to treat aneurysmal bulge A. Staked patch 72 includes a patch 70, made of Dacron or PTFE for example, and an elongated member 71 secured to the patch. When
30 staked patch 72 is secured into position (by sutures or the like) over the surface of aneurysmal bulge A, elongated member 71 pushes on the aneurysmal tissue

region. Staked patch 72 pushes bulge A into the heart chamber. This pushing likely will result in an even further reduction in the stresses experienced by the adjacent heart wall due to the reduction in the radius of curvature resulting from drawing adjacent regions in toward each other when the patch is in place. Such further reduction in stress would tend to promote a more organized healing of the scar tissue region and prevent progression of the scar into other healthy myocardium. Additionally, by pushing the bulge into the chamber space, thrombosis is less likely to occur because of the active blood flow past the surface of the bulge.

As shown in Figure 49b, staked patch 72 has a single stake 71 secured to the patch in a substantially perpendicular direction. However, it is contemplated that several stakes could be secured to the patch depending on the size of the affected tissue area to be treated. Additionally, stakes could be secured in various orientations, including skewed orientations, relative to the patch. The stakes have different sizes in order to optimize the degree and direction in which the bulge is pushed in, especially when the bulge has a non-uniform surface configuration. The stakes may be rigid or semi-rigid and may be manufactured from implantable metals and polymers, or other suitable materials of similar characteristics.

A three-dimensional patch also is contemplated by the present invention. Such a patch could be inflatable or solid. The patch would consist of an essentially flat surface configured to lie flush with the epicardial surface and a bulging surface that would engage with the aneurysmal region to push the aneurysm into the chamber in a manner similar to the stake described above. A suture ring may be placed around the perimeter of the flat surface to secure the patch into place on the heart.

A further embodiment of the present invention is a shrinkable patch for treating aneurysms. For example, such a patch may be made of heat-shrinkable material and applied via sutures to the aneurysmal tissue region while the tissue is in a relaxed state. Gentle heat, such as that produced by, for example, a hot air gun, an infrared heating lamp, or other similar heating mechanisms, would then

be applied to shrink the patch. This shrinking also will cause the size of the affected area to be decreased by being pulled in tightly with the shrinking patch, thereby reducing the radius of curvature of the adjacent myocardium. The patch may be made of any suitable material compatible with the human body and
5 having heat-shrinking characteristics. Examples of such a material include oriented polyethylene, oriented polypropylene, and a woven Dacron polyester of partially-oriented yarn. Partially-oriented yarn is capable of significant longitudinal shrinkage when heated. Additionally, targeting and heating certain areas yields a non-uniform shrinking that more precisely tailors the resulting
10 configuration of the patch and the affected tissue region.

Another embodiment of the present invention, which may be used either alone or in combination with a patch, is a purse-string suture 50, as shown in Figures 50a-50b. In this embodiment, a suture 50 is placed to encircle the affected tissue area 24, as shown in Figure 50a. Suture 50 has free ends 51 that
15 are pulled to draw in suture 50 and reduce the perimeter of the affected tissue, as shown in Figure 50b. Free ends 51 are then secured so as to keep the gathered tissue region in place. The securing can be accomplished by tying free ends 51 to one another or by some like means. By gathering the infarcted tissue together and reducing the perimeter, tension in the walls adjacent to the infarcted tissue
20 24 decreases due to the reduction in radius of the wall in that region. Thus, improved contractile function of the adjacent tissue is expected. Purse-string suture 50 could be drawn in to such an extent that the outer walls of the perimeter of infarcted tissue 24 contact each other. Drawing the infarcted tissue 24 to this extent cuts off the tissue completely from the rest of the heart chamber
25 and renders it non-functional. In addition to the purse-string suture 50, a patch may be applied to support any bulging tissue area that remains after application of suture 50, as well as provide a more secure means of maintaining the gathered portions of the myocardium.

Figures 51a-51c illustrate a further embodiment of the present invention,
30 the combination of a purse-string suture and an enclosure member 60. In this embodiment, purse-string suture 50 is applied to infarcted or aneurysmal tissue

24 as described above with reference to Figures 50a-50b. After the suture is pulled tight to gather the affected tissue region in, an enclosure member 60 is secured into place. As shown in Figure 51c, enclosure member 60 is placed around the gathered tissue 24 so that substantially all of the infarcted tissue is contained inside enclosure member 60. In a preferred form of the invention, sutures are used to secure the enclosure member 60 into place, however other securing means are also contemplated. Enclosure member 60 preferably is made from a substantially rigid material, for example stainless steel, semi-rigid material, or any other material exhibiting like characteristics such as, for example, polyamide imide, titanium, or ultra high molecular weight polyethelene, in order to carry the load created by the gathered infarcted tissue. Because of its relative rigidity, enclosure member 60 withstands the load of the gathered tissue better than sutures alone and contains the progression of the infarcted tissue. Although Figure 51c shows a ring as enclosure member 60, other shapes may be used to serve the inventive purposes. Overall, regardless of the shape of enclosure member 60, its perimeter should be selected to have approximately the same shape as the perimeter of the infarcted tissue region once it has been gathered together by purse-string suture 50.

Another enclosure device is shown in Figures 52a-52c. Figure 52a shows a region 24 of infarcted myocardium on left ventricle LV. Other heart structure shown in these figures includes the right ventricle RV, the right atrium RA, the superior and inferior vena cavas, and the aorta. The inventive enclosure member 61 of Figures 52a-52c is configured to change from a circular shape to an elliptical or oval shape. Such an enclosure member can be fabricated from a shape memory alloy, such as nitinol, or other similar suitable material, and processed such that it has a circular shape at a temperature below its transformation temperature, which is approximately equal to body temperature. Upon reaching the transformation temperature, the ring, comprised of the shape memory material, alters its configuration to the shape of an ellipse or oval, or other suitable configurations. During surgical application, the temperature of the heart is below body temperature and therefore ring 61 remains in the circular

shape during application of ring 61 to the heart, as shown in Figure 52b. After installation of the ring is complete, the heart reaches normal body temperature, transforming ring 61 into the elliptical or oval shape, as shown in Figure 52c. This shape transformation deforms the infarcted region of tissue on the heart wall to change the shape and/or size of the heart chamber, relieve stress on the heart walls, and improve overall contractile function of the heart. In a preferred embodiment, infarcted region 24 deforms in a short axis direction, as shown in Figure 52c.

Alternatively, enclosure member 61 can be formed of a spring metal, such as, for example, high tensile strength stainless steel. When such a material is used, the enclosure member is initially processed into the elliptical or oval configuration. The enclosure member is then attached around a circular polymer, or other suitable material, sheet to form and maintain a circular shape during attachment of the ring to the ventricle. Once attached, the circular polymer sheet is removed, causing the enclosure member to spring back to its original elliptical shape.

Other embodiments of the present invention include enclosure members that deform non-uniformly, either by having a non-uniform configuration at the shape memory transformation temperature, or at the initial processing shape of the spring metal. It also should be noted that enclosure member 61 can take on any suitable shape both before application and after, depending on such factors as, for example, the particular infarcted region to be treated and the desired final radius of curvature.

Figures 53a-53b illustrate a tie enclosure, a further embodiment of the invention and a variation on the use of the enclosure member. The tie enclosure includes a plurality of sutures 62 having free ends 64. Sutures 62 secure around the perimeter of the infarcted or aneurysmal tissue 24, as shown in Figure 53a. Sutures 62 are secured at points 63 using pledgets 65. Enclosure member 60 is then placed over the affected tissue region and free ends 64 of the plurality of sutures 62 are extended through enclosure member 60 to pull sutures 62 through enclosure member 60 as well. By pulling on free ends 64 of sutures 62, the

infarcted or aneurysmal tissue region 24 is again gathered and its perimeter reduced. The tissue is drawn so that pledgets 65 ultimately are adjacent enclosure member 60. The tissue, attached to the sutures, is drawn through enclosure member 60, and once in place, enclosure member 60 can be sutured to the myocardium. Free ends 64 of sutures 62 are drawn until pledgets 65 are brought close to enclosure member 60. Sutures 62 are then tied to the enclosure member 60. Additionally, enclosure member 60 may be directly sutured to the myocardium, as shown in Figure 53b. Again, drawing in the aneurysmal tissue region reduces stress on the chamber walls, hinders the progression of the infarction, and results in a more uniform scar formation, and reduces the radius of curvature, and therefore the stress, in the region of the chamber adjacent the infarction, as well as more global reduction of radius of curvature.

The tie enclosure also allows for non-uniform drawing in of the affected tissue region by using a plurality of sutures of varying lengths. Thus, the tie enclosure allows for particular regions of the aneurysm or infarction to be targeted and drawn in while others are left intact or drawn in to a lesser degree. This allows for a more precise change in geometrical configuration that may be necessary due to non-uniformities existing in the initial geometry of the infarcted or aneurysmal region. Enclosure member 60 also may be made of a flexible material so as to allow enclosure member 60 to take on a non-uniform configuration when sutures 62 are drawn and secured.

As discussed previously, enclosure member 60 may be made of a rigid, semi-rigid, or flexible material, depending on the particular application for which the device will be used. The shape of enclosure member 60 can be that of a ring as shown in Figures 53a-53b or can be another shape, as long as the perimeter of enclosure member 60 is less than or equal to that of the drawn in tissue region.

Using enclosure member 60 and sutures 62 in the manner described with respect to Figures 53a-53b, wider zones of infarcted or aneurysmal tissue preferentially may be drawn further toward enclosure member 60, thereby maximizing the radius reduction in the direction of the widest dimension. This

enables portions of the ventricle that are the most affected by the infarction to experience the greatest radius reduction and therefore the greatest stress relief.

Yet another form of an enclosure member contemplated by the present invention is illustrated in Figure 54. Enclosure member 65 in Figure 54 takes the form of a braided ring with a lumen through which tightening cords 66 extend. Enclosure member 65 can be sutured into place surrounding an infarcted zone of tissue, with the sutures passing through enclosure member 65 only and not through tightening cords 66. Once member 65 is secured around the infarcted tissue, tightening cords 66 can be pulled to draw in enclosure member 65, causing the infarcted tissue region to be drawn together to thereby reduce the radius of curvature of the heart wall in that location. Enclosure member 65 may be made of a relatively flexible material that is either atraumatic itself or is wrapped in an atraumatic material such as Dacron or PTFE for example. Other materials that encompass these characteristics are considered to be within the scope of this invention as well.

In treating infarcted tissue and aneurysms with the various inventive methods and devices discussed above, it may be necessary to identify and distinguish between the infarcted tissue regions of the chamber wall and the contractile tissue regions of the chamber wall. Thus, a further aspect of the invention consists of the use of various devices for performing such identification in order to achieve precise placement of the inventive devices, including the splints, sutures, patches, and rings. The identification devices can be used either endocardially, epicardially, or transcardially, depending on which treatment procedure is being performed.

One such method of identifying infarcted tissue regions from contractile tissue regions involves the use of a bipolar electrode. Using the electrode, differences in impedance sensed by the electrode will indicate regions of infarcted versus contractile tissue.

Another method involves the use of fiber optics to distinguish infarcted from contractile regions of tissue. In this case, the fiber optics sense either density or color differences in transmitted or reflected light. Such differences

would indicate whether a region contained infarcted tissue or contractile tissue. For instance, a known intensity of light could be directed toward a tissue region, with a known nominal intensity transmitting through contractile tissue regions. Intensities of the transmitted light through the chamber wall could then be
5 measured. Upon sensing a decrease in intensity from the nominal value, the infarcted region could be pinpointed. Border zones also could be sensed in this way by looking for a gradation in transmission differences from the nominal value to a lowest value.

Another method to locate regions of infarcted versus contractile tissue can
10 be employed during the surgical procedure itself. This method involves the injection of radioactive media, such as in a thallium scan, with "real-time" imaging of the radiation during the surgery through the use of a Geiger counter contact probe. Higher observed radiation densities indicate regions of perfused tissue. Yet another injection method uses a visible dye injected into coronary
15 vessels to identify contractile perfused tissue. In this identification technique, the dye travels only to contractile tissue, not to infarcted or scarred tissue regions. Finally TEE, or transesophageal echo ultrasounds may be used to detect regions of infarcted tissue.

Aside from those listed above, other methods are contemplated to locate
20 infarcted tissue regions. For example, the surgeon may use his fingers to probe the outer surface of the chamber wall and feel for differences in the tissue regions.

All of the inventive passive devices to be implanted in the heart may be made of biocompatible material that can remain in the human body indefinitely.
25 Any surface engaging portions of the heart should be atraumatic in order to avoid tissue damage.

It will be understood that this disclosure, in many respects, is only illustrative. Changes may be made in details, particularly in matters of shape, size, material, number and arrangement of parts without exceeding the scope of
30 the invention. Accordingly, the scope of the invention is as defined in the language of the appended claims.

Other embodiments of the invention will be apparent to those skilled in the art from consideration of the specification and practice of the invention disclosed herein. It is intended that the specification and examples be considered as exemplary only, with a true scope and spirit of the invention being indicated by the following claims.

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